

AUTOMATIC SEGMENTATION AND CARDIOPATHY CLASSIFICATION IN CARDIAC MRI IMAGES BASED ON DEEP NEURAL NETWORKS

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ABSTRACT

Programmed absconds recognition in MR pictures is significant in numerous demonstrative and remedial applications. In light of high amount information in MR pictures and obscured limits, tumor division and order is hard. This work has presented one programmed Heart sickness identification strategy to expand the exactness and yield and abatement the finding time. The objective is grouping the tissues to three classes of normal, begin and malignant. In MR pictures, the measure of information is a lot for manual understanding and examination. During recent years, Heart ailment division in attractive reverberation imaging (MRI) has become a rising examination territory in the field of clinical imaging framework. Exact identification of size and area of Heart ailment assumes an imperative job in the determination of ailment. The conclusion technique comprises of four phases, pre-handling of MR pictures, include extraction, and arrangement. After histogram adjustment of picture, the highlights are extricated dependent on discrete wavelet change (DWT). In the last stage, Convolution Neural Network (CNN) are utilized to arrange the Normal and unusual Heart. An effective calculation is proposed for Heart illness identification .

Keywords: Cardiac MRI, cardiopathy diagnosis, convolutional neural networks, automatic segmentation.

1. INTRODUCTION

Cardiovascular diseases are more cause of death in worldwide. every year 17.3 million deaths are caused by cardiovascular because of this more people place importance on the cardiopathy diagnosis and prevention. for cardiovascular diagnosis Cardiac MRI offers key information by enabling quantitative assessment

of functional parameters such as myocardium thickness, volume of LV and RV. Thus, cardiac MRI segmentation has become an emerging medical imaging issue. the special characteristics of cardiac MRI, heart segmentation is a challenging task. Many existing methods only segment LV or RV but segmentation of both LV and RV is required for some diseases like hypertrophic cardiomyopathy, and abnormal right ventricle. In recent years, with the advent of deep learning methods, more and more researchers have been trying deep learning on cardiac MRI segmentation. performed RV segmentation using convolutional neural networks (CNN) offer detected its location . we propose automatic segmentation and cardiopathy classification in cardiac MRI images based on deep neural networks. we perform automatic segmentation of LV cavity, RV cavity and myocardium . Next, we extract features such as Energy, Contrast, Correlation, Homogeneity, Entropy from the segmentation mask, and finally classify heart by a CNN whether its normal or abnormal. By clustering the tumour part we can detect the volume of tissue.

2.METHODOLOGY

In this proposed system, first to process the input image Preprocessing is used to improve the quality of an image. To remove the noise and blurriness using Median filter. DWT used to detect the Tumor in heart images. The image can be segmented thoroughly and finally the image into segments. Then, classification is done after features extracted from the input image.

2.1 DISCRETE WAVELET TRANSFORMATION

In numerical examination and useful investigation, a discrete wavelet change (DWT) is any wavelet change for which the wavelets are

discretely inspected. Wavelets are regularly used to denoise two dimensional signs. The two-dimensional wavelet change is distinguishable, which implies we can apply an one-dimensional wavelet change to a picture. We apply one-dimensional DWT to all lines and at that point one-dimensional DWTs to all segments of the outcome. This is known as the normal decomposition. We can likewise apply a wavelet change in an unexpected way. Assume we apply a wavelet change to a picture by lines, at that point by sections, yet utilizing our change at one scale as it were. This procedure will deliver an outcome in four quarters: the upper left will be a half-sized adaptation of the picture and the other quarter's high-pass sifted pictures. These quarters will contain even, vertical, and inclining edges of the picture. We at that point apply a one-scale DWT to the upper left quarter, making littler pictures, etc. This is known as the nonstandard disintegration.

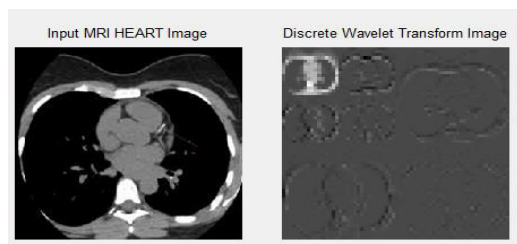


Fig 1. Input image after DWT

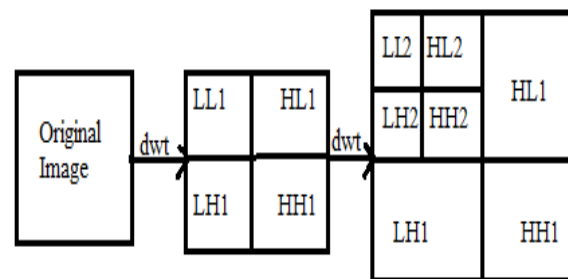


fig 2. Subbands of 2D wavelet coefficients after the first and the second DWT of an image

1. The low-pass/low-pass picture (LL)
 2. The low-pass/high-pass picture (LH)
 3. The high-pass/low-pass picture (HL)
 4. The high-pass/high-pass picture (HH)
- These pictures can be put into a solitary picture framework.

the essential dwt deterioration ventures for a picture in a square outline structure. The two-dimensional DWT prompts a deterioration of picture into four parts CA, CH, CV and CD,

where CA are estimate and CH, CV, CD are subtleties in three directions (level, vertical, and corner to corner), these are same as LL, LH, HL, and HH. We can also collect the important edge details from the input image called edge detection. The automatic segmentation is done in the DWT.

2.2 GRAY LEVEL CO-OCCURANCE MATRIX

The surface channel capacities give a measurable perspective on surface dependent on the picture histogram. These capacities can give valuable data about the surface of a picture yet can't give data about shape, i.e., the spatial connections of pixels in an image. Another factual technique that considers the spatial relationship of pixels is the dim level co-event framework (GLCM), otherwise called the dim level spatial reliance lattice. The tool kit gives capacities to make a GLCM and get factual estimations from it the co-event framework portrayal of surface highlights investigates the dark level spatial reliance of texture. To make a GLCM, utilize the graycomatrixwork. The graycomatrix work makes a dark level co-event grid (GLCM) by ascertaining how regularly a pixel with the force (dim level) esteem I happens in a particular spatial relationship to a pixel with the worth j. As a matter of course, the spatial relationship is characterized as the pixel of intrigue and the pixel to its quick right (on a level plane neighboring), yet you can indicate other spatial connections between the two pixels. Every component (i,j) in the resultant glcm is just the aggregate of the occasions that the pixel with esteem I happened in the predefined spatial relationship to a pixel with esteem j in the info picture. At first the co-occurrence matrix is constructed, based on the orientation and distance between image pixels. Then meaningful statistics are extracted from the matrix as the texture representation. Haralick proposed the texture feature are Energy, Contrast, Correlation, Homogeneity. Consequently, for each Haralick surface element, we get a co-event framework. These co-event lattices speak to the spatial dispersion and the reliance of the dim levels inside a neighborhood. Each (i,j) th section in the frameworks, speaks to the likelihood of going from one pixel with a dim degree of 'I' to

another with a dim degree of 'j' under a predefined separation and edge. From these grids, sets of factual measures are figured, called highlight vectors.

Energy : It is a dim scale picture surface proportion of homogeneity changing, mirroring the dissemination of picture dim scale consistency of weight and surface.

$$E = \sum \sum p(x, y)^2 \quad P(x, y) \text{ is the GLCM} \dots\dots(1)$$

Contrast: Contrast is the primary corner to corner close to the snapshot of latency, which measure the estimation of the lattice is circulated and pictures of neighborhood changes in number, mirroring the picture clearness and surface of shadow profundity.

$$\text{Contrast } I = \sum \sum (x-y)^2 p(x,y) \dots\dots(2)$$

Correlation Coefficient: Measures the joint likelihood event of the predetermined pixel sets.

$$C = \sum \sum ((x - \mu_x)(y - \mu_y)p(x, y) / (\sigma_x \sigma_y)) \dots\dots(3)$$

Homogeneity: Measures the closeness of the conveyance of components in the GLCM to the GLCM askew.

$$H = \sum \sum (p(x, y) / (1 + |x-y|)) \dots\dots(4)$$

Entropy: It estimates picture surface arbitrariness, when the space co-event framework for all qualities is equivalent, it accomplished the base worth.

$$S = \sum \sum p(x, y) \log p(x, y) \dots\dots(5)$$

2.3 CONVOLUTION NEURAL NETWORK

Normally the classification is used to classify that the image is normal or abnormal. NN is one type of classifier, the features and values of the tumor affected image and non tumor image is already placed in database, the intensity is also having in tumor affected image, the classifier compares the given image within the database if the tumor is identified while comparing the each pixels. A convolution neural system can have tens or several layers that each figure out how to identify various highlights of a picture. CNN is made out of an info layer, a yield layer, and many concealed layers in the middle. These layers perform tasks that adjust the information with the aim of learning highlights explicit to the information. Three of the most widely recognized layers are: convolution, Activation or ReLU, and pooling.

Convolution: gets the info pictures through a lot of convolution channels, every one of which enacts certain highlights from the pictures.

(ReLU): Rectified linear unit, considers quicker and progressively viable preparing by planning negative qualities to zero and keeping up positive qualities. This occasionally alluded to as initiation, in light of the fact that solitary the actuated highlights are conveyed forward into the following layer.

Pooling: improves the yield by performing nonlinear down sampling. Reducing the quantity of boundaries that the Network needs to learn. These tasks are rehashed more than tens or Hundreds of layers, with each layer figuring out how to recognize various highlights.

Characterization Layers: also known as classification layer. Subsequent to learning highlights in numerous layers, the Design of a CNN movements to Classification. The close to last layer is a completely associated layer that yields a vector of K measurements where K is the quantity of classes that the system will have the option to anticipate.

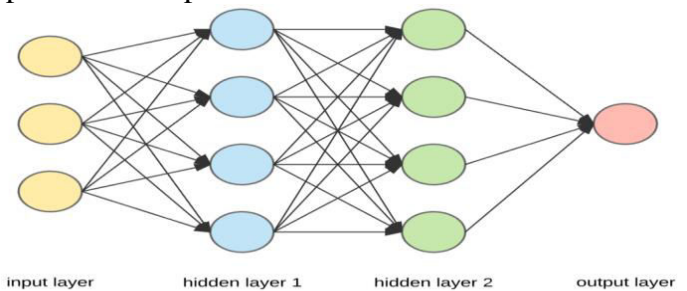


Fig 3. Convolution Neural Network

2.4 FUZZY C-MEANS AND MORPHOLOGICAL PROCESS

In this framework, we can take 4 group, the boundaries for bunching process are type for the segment network, worst case scenario. number of cycle, min. measure of progress. Spatial Fuzzy C Means technique fuses spatial data, and the enrollment weighting of each group is adjusted after the bunch dispersion in the area is thought of. The main pass is equivalent to that in standard FCM to figure the enrollment work in the phantom area. In the subsequent pass, the enrollment data of every pixel is planned to the spatial space and the spatial capacity is processed from that. The FCM cycle continues with the new participation that is consolidated with the spatial

capacity. The cycle is halted when the most extreme distinction between group focuses or enrollment capacities at two progressive emphases is not exactly a least limit esteem.

$$J(wqk, z(k)) = \sum_{k=1}^K \sum_{q=1}^K \|x(q) - z(k)\|^2 \dots (6)$$

$$\sum_{k=1}^K (wqk) = 1 \dots (7)$$

$$wqk = \frac{1}{(\sum_{k=1}^K (Dqk)^{2/(p-1)})^{1/(p-1)}}, p > 1 \dots (8)$$

The FCM permits each component vector to have a place with each bunch with a fluffy truth esteem (somewhere in the range of 0 and 1), which is registered utilizing Equation The calculation allots a component vector to a group as indicated by the greatest load of the element vector over all bunches.

Morphological preparing is a variety of non-straight exercises related to the shape or morphology of features in an image .Morphological procedures test an image with a little shape or design called an arranging component. A morphological system on an equal picture makes another twofold picture where the pixel has a non-zero worth specifically if the test is viable at that territory in the data image.The most essential morphological exercises are extension and disintegration. Expansion adds pixels to the furthest reaches of articles in an image, while breaking down empties pixels on object boundaries.The number of pixels included or removed from the things in an image depends upon the size and condition of the sorting out part used to process the image.

3.PROPOSED BLOCK DIAGRAM

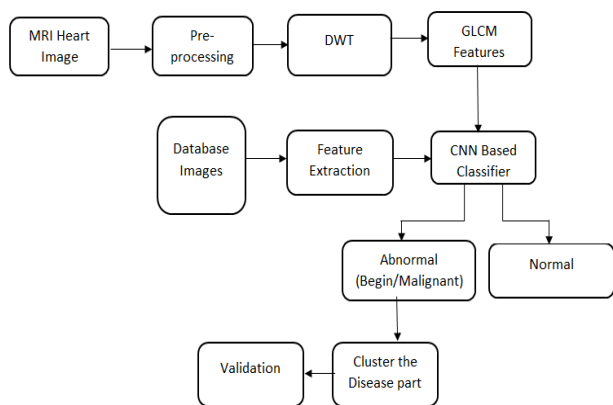


Fig 4. Proposed block diagram

4.SIMULATION RESULTS

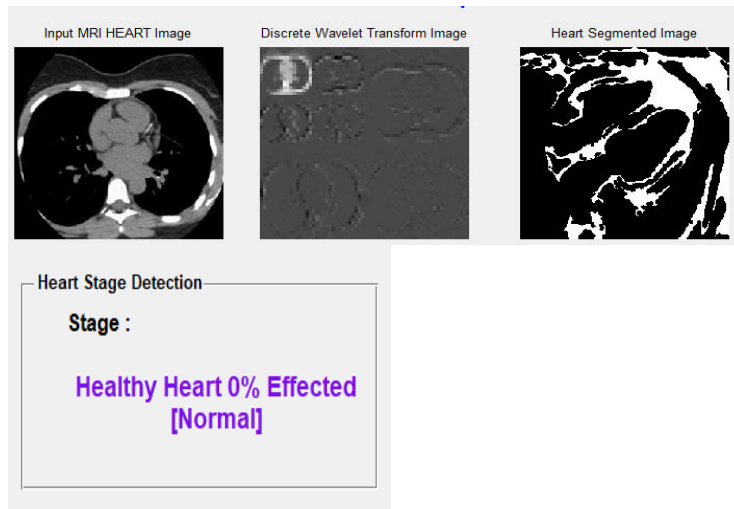


Fig 5. Heart is normal after classification and segmentation

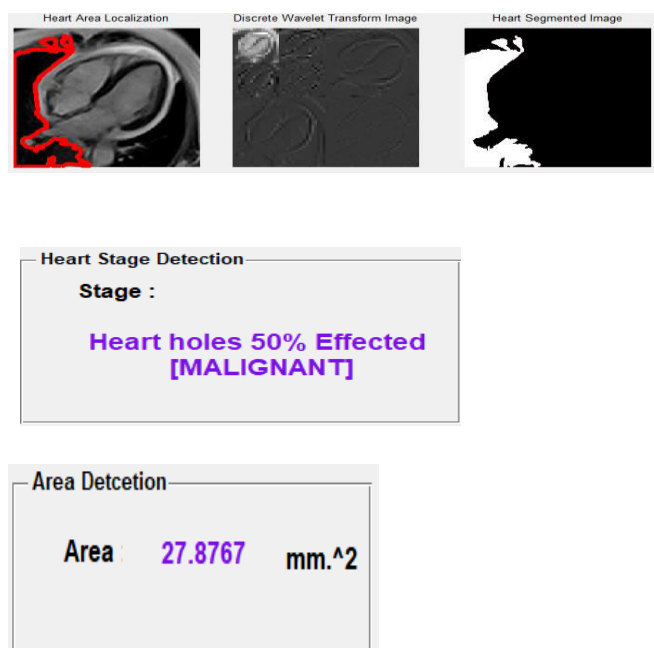


Fig 6. Heart is abnormal(malignant) after classification and Segmentation and heart is 50% effected.

5. CONCLUSION

We simultaneously segment LV cavity,RV cavity and myocardium using a CNN.We perform cardiopathyclassification for heart disease diagnosis with the cardiacsegmentation. Wedevelop a fully automatic method for cardiac MRI segmentation andcardiopathy diagnosis based on deep

neural networks and also to develop the performance of the automatic segmentation of cardiac structures on the detected ROI in order to produce a good segmentation results close to the ground truth, which provides a promising solution to diagnosing cardiopathy from cardiac MRI.

6. REFERENCES

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